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# **Original Article**

# Function and Viability of Vessels in Different Preservation Solutions - An Experimental Study on Human Great Saphenous Veins

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## Abstract

#### Objective

Great Saphenous Veins (SVs) are widely used in coronary and in non-coronary surgery, and the need for vascular transplants is increasing. In older pre-servation solutions, hypothermia leads to damage induced by reactive oxygen species. Iron chelators in the newer Tissue Protection (TiProtec) solution shall par-ticularly protect vessels by preventing from that damage.

It was the aim to compare three preservation solutions to maintain function and viability of human SVs.

#### Methods

Vein segments were randomly assigned to Krebs-Henseleit Buffer (KHB), Viaspan (UW), or TiProtec. Contraction/relaxation in organ baths was assessed at 3, 24, 48 and 72h after removal. The protocol included three steps: receptor-independent contraction (KCI:  $80\mu M$ ), receptor-dependent contraction (PE:  $\leq \! 30\mu M$ ), endothelium-dependent relaxation (ACh:  $\leq \! 20\mu M$ ). Morphology: Vein segments were incubated with propidium iodide and 5-chloromethylfluorescein diacetate. Viability was assessed with fluorescence using laser scanning microscopy.

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#### Results

KHB was inappropriate after only 3h. In TiProtec, SVs contraction/relaxation had increased further at 72h, but not in both other groups. More necrosis was found in KHB SVs than in UW or TiProtec at 3h. More viable cells were found in UW and in TiProtec SVs on day-1, while only few cells were viable in KHB on day-10.

#### Summary and conclusion

Even short storage of SVs in KHB is deleterious. UW preserved func¬tion better over time. The best functional and morphological results yielded TiProtec over time, and the amount of viable cells correlated with function. TiProtec seems a promising alternative for short- and mid-term hypothermic vein preservation.

**Keywords:** Hypothermia; Iron chelators; Preservation; Reactive oxygen species; Transplantation; Vessel

#### Introduction

In the last decades blood vessel transplantation and preservation have grown steadily in importance. Although storage of those vessels induces injury, mechanisms of injury due to cold storage have only recently been extensively studied. Injury due to cold storage and prevention from injury have already been exhibited for corneal cells, cultured endothelial cells, hepatocytes, rat mesenteric artery, segments of rat and pig aorta and lung epithelial cells [1-3]. The same is true for the human internal thoracic artery [4]. On the other hand, preservation solutions themselves can develop an inherent toxicity upon rewarming [5-7].

A number of studies have shown that hypothermia injury results from a growing pool of redox-active iron [8,9]. The iron mediates the formation of Reactive Oxygen Species (ROS) which in turn lead to lipid peroxidation, changes in mitochondria, and finally to cell death [10]. The rewarming when the tissue is transplanted exacerbates this process while iron chelators were shown to ameliorate the damage [1].

Presently used preservation solutions, developed in the early 1980's, do not take cold-induced damage into account. These older solutions include Histidine-Tryptophan-Ketoglutarate (HTK) solution (Custodiol) and University of Wisconsin solution (Viaspan). HTK solution was the basis of the newer Tissue Protection (TiProtec) solution that was specially developed [4] for the preservation of blood vessels and therefore contains iron chelators.

Despite the growing need for vascular transplants, methods of preservation are not stringently established. The necessity for a preservation solution that is optimized for blood vessels becomes apparent from a recent retrospective study [11], which reports on a re-occlusion rate of 25% 12-18 months after an aorto-coronary bypass operation. Causes of this problem are damage during preparation, unfavorable conditions of inflow or outflow in the region of the anastomosis, turbulences if vessel diameter is too small, and damage to the endothelium [12]. The protection of endothelial function is particularly important in preventing postoperative thrombosis and stenosis [13]. Some authors [14,15] view transplant failure as the long-term consequence of intima hyperplasia, which results from multifactorial damage to the endothelium.

The great Saphenous Vein (SV) is a well-established preparation for autologous and allogenic vein grafts [16]. It serves as a bypass in cardiovascular procedures and for reconstruction or patch in vascular surgery. The SV is employed worldwide with more than 80% of all surgical heart procedures for myocardial revascularization performed with autologous vein grafts [17,18]. However, 25% of these vein conduits are already occluded after 1 year of surgery, and almost 75% are occluded 10 years after surgery [19]. It is easily conceivable that the results become even worse if SV need to be stored before allogenic usage. Thus, optimized preservation solutions for most appropriate storage are essential.

Both function and histology will be addressed in this study. Thus, some histological properties of the great saphenous vein are given: It has a thin intima covered by endothelium, which is separated from the media by a rudimentary internal elastic lamina. The media consists of a less prominent inner layer of longitudinal muscle fibres and a more prominent outer layer of circular muscle fibres. The adventitia is composed of connective tissue and contains the vasa vasorum [20].

The present study was designed to test the hypothesis that TiProtec preserves both function (i.e., smooth muscle contractility in an organ bath) and viability (as judged by confocal laser microscopy) of human SV better than the older Custodiol solution and the Viaspan solution.

#### **Material and Methods**

Veins were taken from patients at the University Clinic Düsseldorf who underwent an Aorto-Coronary Venous Bypass operation (ACVB). In the course of this operation a piece of the great Saphenous Vein (SV) was removed from the leg. Left-over pieces of vein were kept in physiological saline until the end of the operation, after which they could be used for the purposes of this study.

Patients gave their informed consent to the use of their left-over veins for experimental purposes. The Ethics Commission of the Medical Faculty of the Heinrich-Heine-University Düsseldorf had approved the study. Previous illnesses, medication, BMI, age and sex were recorded for each patient (Table 1). No exclusion criteria were specified in advance, except for clearly recognizable varicosis.

Number of patients	77			
Sex (%; females/males)	27/73			
Age [years; mean ± SD]	67.1 ± 15.4			
BMI [kg • m <sup>-2</sup> ; mean ± standard deviation]	30.3 ± 7.6			
Table 1: Demographic data of the vessel donors				

In the laboratory of the Research Group Experimental Surgery the SV were carefully cut into segments at least 4 mm wide on a cooled rubber surface. Surrounding fatty tissue was removed. During these procedures veins were immersed in Krebs-Henseleit (KH) buffer. A vein segment was discarded if it did not develop an initial tension of at least 3.0 mN under KCl. Vein segments were then stored at 4°C for up to 72 h in one of the preservation solutions under study.

#### **Preservation solutions**

The KH buffer was prepared fresh each day. It was titrated to pH 7.2 at 37.0°C using 1 M hydrochloric acid [21]. Carbogen (95% O<sub>2</sub> / 5% CO<sub>2</sub>) bubbled through the solution raised pH to 7.4 (veins are very sensitive to variations in pH).

The University of Wisconsin (UW) solution (Viaspan; Bristol-Myers Squibb GmbH & Co. KGaA, München, DE) is comparatively viscous (4.8 cP at 4°C). Its pH at room temperature is 7.4. The solution is clear, colorless to yellow, and stored under aseptic conditions, with 16 mg dexamethasone, 40 IU insulin and 200.000 IU penicillin G added for organ preservation (information provided 2005 by the manufacturer Bristol-Myers Squibb Pharmaceuticals).

The TiProtec solution (Köhler Chemie GmbH, Bensheim, DE) (Table 2) was developed on the basis of the proven Histidine-Tryptophan-Ketoglutarate (HTK) solution (Köhler Chemie GmbH, Bensheim, DE). It contains two different iron chelators: deferoxamine (0.1 mM Desferal), which does not permeate the cell membrane, and LK614 (20 μM), which does. In TiProtec histidine is replaced by acetylhistidine, which has a modified affinity to iron and is thus less toxic.

Ingredient	Concentratio (mM)	
CI <sup>-</sup>	103	
α-ketoglutarate	2	
aspartate	5	
H₂PO4 <sup>-</sup>	1	
Na⁺	16	
K+	93	
Mg²+	8	
Ca²+	0.05	
tryptophane	2	
saccharose	30	
N-acetylhistidine	30	
glycine	10	
alanine	5	
glucose	10	
deferoxamine	0.082	
LK 614	0.017	
pH (20°C)	7.0	
osmolarity (mosm/l)	305	

Table 2: TiProtec solution; 100 ml solution contains the following.

#### Function

Veins were stored at 4°C. They were randomly assigned to three groups and placed in organ baths (Föhr Medical Instruments GmbH, Seeheim-Ober Beerbach, DE) for testing contraction and relaxation. The solution in the control group contained KHB (n=26); experimental groups contained either UW solution (n=26) or TiProtec (n=25).

Function of the veins was studied at intervals of 3, 24, 48 and 72 h after preservation began. After each interval, veins were carefully rinsed three times from inside and outside with KHB and warmed within 30 min to 37°C. After the function tests, veins were placed in cooled opaque Eppendorf pipettes in fresh preservation solution and refrigerated at 4°C until the next test.

Initial tension of vein segments was adjusted to  $12.5 \pm 0.4$  mN; it took 20 to 40 min to achieve stable tension for 3 min, after which testing began. If necessary, initial tension was reset between tests.

The following protocol was used in testing veins: 1) receptor independent contraction (80 µM KCl), 2) receptor dependent contraction (cumulative in steps up to 30 µM phenylephrine; Sigma-Aldrich Chemie GmbH, München, DE), 3) endothelium

dependent relaxation (cumulative in steps up to 30  $\mu M$  acetylcholine; Sigma-Aldrich Chemie GmbH, München, DE).

# Morphology

In the second part of the study, viability and necrosis of endothelial and smooth muscle cells were assessed over a period of 10 days.

Viable cells were visualized using CellTracker Green (5-chloromethylfluorescein diacetate; CMFDA; Invitrogen, Carlsbad, DE). Living cells containing CMFDA fluoresce in green. In order to visualize necrotic cells, vein segments were incubated with membrane impermeable propidium iodide (Sigma-Aldrich Chemie GmbH, München, DE). After cell death propidium iodide can enter a cell and intercalate with DNA, leading to red fluorescence under an argon laser.

Fluorescence was tested at 1 and 10 days after removal using a laser scanning microscope (LSM510, Axiovert 100M; Zeiss, Jena, DE). Veins were cut at room temperature in a Petri dish to a size of  $0.3\times0.5$  cm. The quality of the stain was checked at  $\times10$  magnification. Then at  $\times40$  magnification the relation of viable to necrotic cells was assessed layer by layer in 7.5  $\mu m$  steps in order to differentiate endothelium (intima) from smooth muscle (media). Two veins were processed in this way for each of the three preservation solutions. An external observer blinded to the study protocol performed the observations.

#### **Statistics**

Raw data were protocolled using a computer and transferred to an Excel spread sheet. Three independent persons checked the data before they were transferred to the program used for statistical analysis (SPSS, Version 19; SPSS Inc, Chicago, US).

An Analysis of Variance (ANOVA) was performed after a check for normal distribution of data with the Kolmogorov-Smirnov test. The Greenhouse-Geisser correction for repeated measures was used; it leads to more conservative values, which were used in all subsequent analyses. In case of significant effects, a post-hoc Scheffé test was used for individual comparisons. Paired t-tests were used to compare initial and final values. Results with p < 0.05 were considered significant.

#### Results

A total of 91 patients that were scheduled for routine coronary artery bypass surgery donated vein grafts. Of these, 14 were discarded because they exhibited clearly recognizable signs of either surgical injury or varicose. Thus, 77 vein segments could be included into the study. Initial tests were conducted on the vein segments after 3 h storage in one of the preservation solutions. Already at this step there was a marked difference between the solutions. Only 15/26 (58%) of the veins in KH buffer were suitable for further testing. In contrast, 18/26 (69%) of those in UW solution and 19/25 (76%) in TiProtec could be used for further tests.

### Receptor independent contraction using KCl

After 3 h (Figure 1) veins preserved in KH buffer were already slightly weaker (20.1  $\pm$  3.5 mN; mean  $\pm$  standard deviation) than those in the UW group (29.1  $\pm$  7.3 mN) and significantly weaker than those preserved in TiProtec (41.4  $\pm$  16.2 mN). After 72 h in KH buffer no contraction stronger than 12 mN could be induced using KCl. The standard deviation got smaller as preservation time increased, indicating that contractile vein function decreased uniformly in KH buffer.

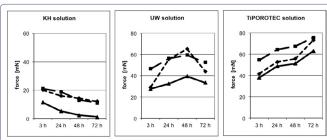


Figure 1: Contraction induced by Potassium Chloride (KCI) and Phenylephrine (PE) and relaxation by Acetylcholine (ACh). Human great saphenous vein rings were protected either in Krebs-Henseleit solution (KH), or in University of Wisconsin solution (UW solution; Viaspan), or in TiProtec solution.

KCI: solid line; phenylephrine: dashed line; ACh: dash dotted line

For clarity, no standard deviation and significance symbols are presented. Please, see Results.

In the UW group function increased significantly up to 48 h, reaching 65.0  $\pm$  31.0 mN, but it had decreased again after 72 h (43.9  $\pm$  17.3 mN). After 24 h the UW solution was significantly better than KH buffer (55.2  $\pm$  18.1 vs. 16.0  $\pm$  5.8 mN).

In the TiProtec group contractile force increased steadily from 41.4  $\pm$  16.2 mN after 3 h, to 73.0  $\pm$  31.9 mN after 72 h, an overall increase of 76%. After 72 h vein segments in the TiProtec contracted significantly stronger (Table 3) than either the segments of the KH group (12.0  $\pm$  0.9 mN) or those of the UW group (43.9  $\pm$  7.3 mN).

		KH buffer n=9	UW solution n=11	TiProtec n=12
		mean ± SD [mN]	mean ± SD [mN]	mean ± SD [mN]
Potassium Chloride (KCI)	3 h	20.1±3.5+	29.1±7.3	41.4±16.2
	24 h	16.0±5.8*°+	55.2±18.1*	52.6±29.3
	48 h	14.3±2.8*°+	65.0±31.0*	55.5±28.0
	72 h	12.0±0.9*°+	43.9±17.3⁺	73.0±31.9
Phenylephrine	3 h	21.0±5.2°+	46.4±13.3	54.6±17.8
	24 h	18.7±7.1°+	56.2±16.7	64.2±28.6
	48 h	12.8±1.0*°+	59.6±15.3	67.4±29.7
	72 h	11.0±2.3*°+	52.4±20.6⁺	75.5±23.6
Acetylcholine	3 h	11.4±5.3°+	27.6±9.9	38.1±15.1
	24 h	5.2±4.6*°+	32.5±12.7*	48.7±30.5
	48 h	2.2±1.0*°+	39.5±16.5	51.2±28.3
	72 h	1.0±0.7	33.4±16.7°+	63.0±21.8

Table 3: Contraction induced by KCl and PE and relaxation by ACh.

Data are mean ± Standard Deviation (SD)

\*p < 0.05 vs preceding time point; \*p < 0.05 vs UW solution; \*p < 0.05 vs TiProtec

# Receptor dependent contraction using Phenylephrine (PE)

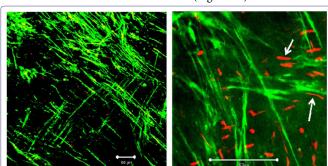
Increasing the PE dosage cumulatively from 0.3  $\mu$ M to 30  $\mu$ M induced a maximal  $\alpha$ -receptor contraction of the segment. The results in this part of the experiment were comparable to those on receptor independent contraction. After 3 h the contraction force of vein segments was significantly lower in the KH buffer than in either of the other two groups: 21.0  $\pm$  5.2 mN as compared to 46.4  $\pm$  13.1 mN (UW) and 54.6  $\pm$  17.8 mN (TiProtec). The differences remained significant at each of the later times (Table 3). As was the case using KCl, contractile force in the TiProtec group increased steadily, while it

slightly decreased in the UW group after 48 h (Table 3). After 72 h TiProtec was significantly superior:  $75.5 \pm 23.6$  mN as compared to  $11.0 \pm 2.3$  mN (KH buffer) and  $52.4 \pm 20.6$  (UW solution).

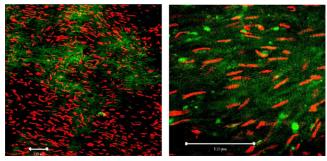
# Endothelium dependent relaxation using Acetylcholine (ACh)

The behavior of the vein segments during relaxation from maximal contraction (30  $\mu M$  PE) was comparable to what was observed in the contraction series. The ability of veins in KH buffer to relax decreased steadily with time (Table 3) from 11.4 mN (3 h) to 1.0 mN (72 h). Relaxation was significantly better at all times in the other two groups. After 72 h, relaxation of veins in the TiProtec group was better than in the UW group (63.0  $\pm$  21.8 mN as compared to 33.4  $\pm$  16.7 mN).

Morphology. After only 3 h the muscular layer in the KH buffer group appeared somewhat coarser and more loosely packed compared to the other two groups, and more necrotic cells were found, mostly of endothelial origin (Figure 2A). After 10 days there were almost no viable cells or coherent tissue to be seen (Figure 2B).



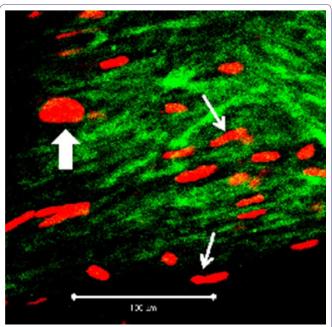
**Figure 2A:** Segment of vein from the KH group on day 1. Left: X10 magnification; white bar: 100  $\mu$ m, right: detail (X40 magnification; white bar: 100  $\mu$ m). White arrows: smooth muscle cell.



**Figure 2B:** Segment of vein from the KH group on day 10. Left: X10 magnification; white bar:  $100 \ \mu m$ , right: detail (X40 magnification; white bar:  $100 \ \mu m$ ). Compared to first day (Figure 2a) red fluorescence (= necrotic cells) has clearly increased.

In the UW group myocytes also appeared to be more loosely packed and necrotic endothelial cells were found after 10 days cold storage (Figure 3), but not to the extent seen in the veins in KH buffer. The structure of the venous wall was partially loosened, but it was very much better preserved than in the veins of the KH group. Thus, stable contraction and relaxation behavior was still observed up to 48 h. There was no difference between the UW and TiProtec groups on day 1, with viable cells clearly forming a coherent tissue (Figure 4).

Even after 10 days in TiProtec no coarsened matrix was observed and the number of necrotic endothelial cells was noticeably fewer than in either of the other two groups (Figure 5).



**Figure 3:** Segment of vein from the UW group on day 10 (detail at X40 magnification; white bar:  $100~\mu m$ ). Viable cells fluoresce in green, apoptotic cells in red. Heavy arrow: PI-positive endothelial cell, thin arrows: PI-positive myocytes.

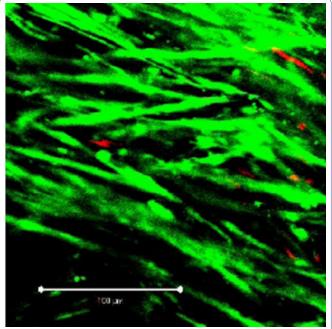
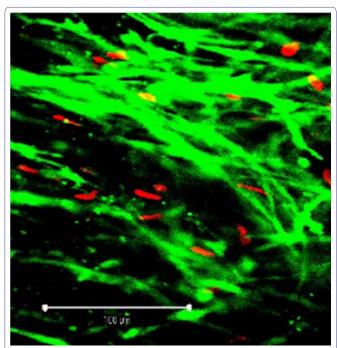


Figure 4: Segment of vein from the TiProtec group on day 1 (detail at X40 magnification; white bar:  $100 \ \mu m$ ).

## Discussion

It is the main finding of this experimental study on human saphenous veins that the newer preservation solution (TiProtec), especially designed for use with blood vessel transplants, proved significantly superior to either KH buffer or UW solution in the KCl contraction test after only 3 h preservation. Thus, TiProtec appears well suited for short-term preservation (e.g., in bypass operations). On the other hand, KH buffer does not seem appropriate even for temporary storage in the operating theater. For 1 to 3 days storage,



**Figure 5:** Segment of vein from the TiProtec group on day 10 (detail at X40 magnification; white bar:  $100 \mu m$ ). Only a few PI-positive cells can be seen. Unlike the other 2 solutions, this preservation solution maintains cellular structure (green).

both UW solution and TiProtec give comparably good results compared to KH buffer. From four days preservation or longer, TiProtec is clearly superior.

The present results also exhibit a relation between viable and necrotic cells on the one hand and contraction and relaxation of the veins stored in the three preservation solutions on the other hand. It thus appears that improved cell morphology is the reason for the improved contraction and relaxation behavior under TiProtec. One may expect that a well preserved transplant can minimize the risk of primary failure and later dysfunction after implantation.

#### **Study Limitations**

There are necessarily certain limits to applying the results of organ bath experiments to *in vivo* reality. Nevertheless, the results of earlier studies as well as those presented here clearly show that the results of animal experiments can be applied to human blood vessels.

Although Vasa Vasorum (VV) in saphenous grafts are needed for the nutrition of the vessel wall, the presence of the VV in our three groups was not assessed. However, the density and the distribution of VV had shown to be uniform and not to differ in great and small saphenous veins [22]. Thus, any damage on VV of our saphenous grafts would have affected the results within the three groups to a similar extent, i.e., differences in VV very unlikely can explain the observed differences described for the three different protection solutions.

Because of an average age of  $67.1 \pm 15.4$  years, presence of varicose veins was to be expected and could have affected the results. For such veins, differences in the orientation of the Smooth Muscle Cells (SMC) in the inner and outer wall layers were reported, but the SMC orientation was uniform along the varicose saphenous veins [23] Thus, we do not consider changes in the SMC orientation responsible for the differences found for the protective solutions, in particular, because veins with clearly recognizable varicose had been discarded.

A final drawback of the study could have resulted from the conventional technique of harvesting the vein grafts in this study opposed to the no-touch technique that has been recommended by some groups, because it provided a significantly higher patency [24] and left ventricular ejection fraction [25] at a mean time of 16 years than the conventional technique.

Kopjar and Dashwood [26] focused on a critical aspect of the no-touch vein harvest that presents a major barrier to wide-spread adoption, which being the morbidity of the leg incision. Because all vein grafts in this study were harvested using the conventional technique, different solution-dependent results cannot be explained by different techniques.

Veins are rather small, and during storage they are bathed both inside and out by preservation solution, which means that both inner and outer surfaces are subject to the same oxygen partial pressure [27]. Damage due to hypoxia is thus less pronounced than for blood vessels within large organs. On the other hand normoxia promotes oxidation processes and the formation of free radicals.

Solutions for preserving blood vessels are now expected to maintain good function and morphology for about two weeks. This length of time is required in order to perform the microbiological tests prescribed by the European guidelines and the German tissue bank law [16].

In the present study the ability of a newer extracellular solution (TiProtec) to preserve human Saphenous Vein (SV) was examined for up to 72 h after removal. TiProtec was compared with the clinically established, intracellular University of Wisconsin (UW) solution. The controls were veins stored in Krebs-Henseleit (KH) buffer. Two independent parts of the study were performed to evaluate preservation ability: in the functional part (organ bath) receptor independent and receptor contraction as well as endothelium dependent relaxation were measured. In the morphological part of the study (confocal laser microscopy) cell viability was investigated.

In the following some of the peculiarities of the preservation solutions used in this study are discussed. The functional and morphological results are viewed in connection with the current literature.

Krebs Henseleit (KH) buffer is frequently employed in experiments using organ baths, cell culture or perfusion. Its pH value depends on continuous bubbling of 95%  $\rm O_2$  / 5%  $\rm CO_2$  through the solution. Without this precaution the pH becomes alkaline. The poor results found in this study with this solution might have been due to this factor, since alkaline pH causes serious damage to stored organs [27]. However, the time course of pH was not measured in this study.

The morphology, too, gives an indication of the importance of gassing the solution. Cultured hepatocytes have been preserved in KH buffer both with and without gassing [28]. Without gassing 4 h in cold storage induced considerable cell damage, as documented by the massive increase in the number of necrotic cells seen using Propidium Iodide (PI).

A further reason for the poor results with KH buffer might have to do with the high concentration of redox-active metals [29], which contribute to the development of Reactive Oxygen Species (ROS) during cold storage and subsequent rewarming. This damage mechanism is not observed with normothermic storage at 37°C, such as is required for cell cultures.

Even on day 1 of preservation veins showed slight morphological changes, such as loosened structure and a somewhat higher number of PI-positive cells. On day 10 there were almost no viable cells and necrotic cells dominated in all cell layers. Thus, KH buffer appears unsuitable for the cold storage of veins.

The University of Wisconsin (UW) solution is frequently used for the preservation of abdominal organs. The UW solution belongs to the intracellular solutions owing to its high  $K^+$  (125 mM) and low  $Na^+$  concentration (29 mM). Disadvantages of this solution include endothelial dysfunction [5] and in the case of lung transplants vasoconstriction and reduced compliance.

A major concern in the case of UW solution is the prevention of hypothermia induced cell swelling, which presumably results from inactivation of the Na $^+$ -K $^+$ -ATPase. The ensuing influx of Na $^+$  and Cl $^-$  ions draws water into the cells osmotically. To prevent this, UW solution contains lactobionic acid, raffinose and Hydroxyethyl Starch (HES). Lactobionic acid also acts as a chelator of Ca $^{2+}$  and iron, which has been suggested to contribute to its effectiveness in preserving cell integrity during hypothermic storage. UW solution also contains glutathione, which as an antioxidant has a protective effect on liver transplants [30]. On the detrimental side, however, glutathione has been shown to cause increased endothelial dysfunction in cold storage [31].

The UW solution has proven useful for the preservation of liver, kidney and pancreas among other organs for 8 to 12 h, sometimes as long as 24 h. It is also used for heart transplants. The clinical importance of this solution is thus apparent.

The protective properties of the UW solution are temperature dependent. An inherent toxicity has been observed during the rewarming phase [5-7], which appears to be the result of a cold induced mechanism mediated by ROS [32]. This cold induced damage has been studied morphologically [32]. One hour after rewarming DNA fragmentation and apoptotic changes were observed, along with a 2.5-fold increase in PI uptake, a sign of more necrotic cells. Such damage was alleviated by adding an iron chelator [32].

In the present study, a stable contraction and relaxation behavior was observed up to 48 h after 10 days of cold storage, a result that was likely owing to the well maintained morphology.

The Tissue Protection (TiProtec) solution was specially developed on the basis of the Custodiol-N solution [33], which in turn was derived from the HTK solution (Custodiol) for liver preservation.

As hypoxic damage is of little importance in the case of thin-walled vessels, avoidance of other damage mechanisms was of primary concern in developing TiProtec. One concern was histidine, which serves as buffer in Custodiol but enhances iron formation at high concentrations [2]. For this reason, in TiProtec histidine was replaced by N-acetylhistidine (pK = 7.2), which has a different affinity for redox-active iron and forms more stable complexes [2].

Another concern was the normoxia during hypothermic preservation, which can lead in particular to ROS induced endothelial damage. In order to avoid this source of damage at most, TiProtec contains two different iron chelators: desferoxamine, which is hydrophilic and does not pass through the cell membrane, and LK 614 [34], which being lipophilic easily passes through the membrane.

Comparatively little solution is required for preserving blood vessels. Hence, amino acids and ions can be used effectively to supply energy and regulate osmolarity. For example, replacing lactobionate anions with chloride led to a significantly increased rate of survival of endothelial cells in segments of pig aorta [3], a result that was confirmed using segments of rat aorta and mesenteric artery [35]. By using a high K+ concentration (93 mM), the mitochondrial membrane potential was better maintained [14] and vasoconstriction and EDHF-mediated relaxation were better than under the HTK solution, the extracellular-type solution used as a starting point [35].

A final concern in the design of TiProtec has to do with the amino acids glycine and alanine, which had already proven useful in the Custodiol-N solution for preventing  $Na^+$  influx during hypoxia. These two amino acids were retained in the TiProtec solution for their membrane stabilizing properties, and aspartate and  $\alpha$ -ketoglutarate were added for maintaining the citric acid cycle [36].

Based on its advanced composition, TiProtec has led to excellent experimental results. Segment of pig aorta have been preserved for up to 21 days [3]. With segments of rat aorta and mesenteric artery, potassium induced vasoconstriction, both endothelium dependent and independent relaxation, eNOS expression and endothelial ultrastructure were all significantly better after four days preservation in TiProtec than in HTK solution [34]. Endothelial structure had already been lost after 2 h in HTK solution, a result that underscores the importance of employing the most appropriate preservation solution as early as possible.

Studies of human thoracic artery (ATI) [4] yield similarly positive results, as does the present study using human veins. For ATI, too, vascular tone was better preserved after four days in the TiProtec solution than in either 0.9% NaCl or the HTK solution.

The damage caused by cold storage and rewarming has already been studied morphologically [3]. No matter which preservation solution was used, the number of PI-positive cells was reduced when iron chelators were added. Of the solutions tested, only TiProtec contains iron chelators as part of its formula. As shown in the present study, iron chelators appear able to effectively reduce damage due to ROS, in particular the number of necrotic endothelial cells was definitely lower than in the other two solutions, a finding that is in good agreement with a previous study on human SV segments [17]. The present study shows in addition that TiProtec also very adequately preserves contractile function.

The human great Saphenous Vein (SV) is clearly a representative model of a blood vessel transplant. SV may also be viewed as a simplified model of an organ containing numerous blood vessels, which must be preserved. This is especially true if an intact vascular endothelium is essential to the function of the organ. It should be remembered, however, that veins induce an immune reaction in the recipient, so they must be protected from being rejected after transplantation.

The clinical importance of the TiProtec solution has remained an open question. Currently available results indicate that TiProtec, specifically designed for use with blood vessels, is a good alternative for the short- and long-term preservation of vessels stored in hypothermia. Given the increasing numbers of blood vessel transplantations, not just clinical considerations but also economic aspects are gaining greater importance. Thus, a comprehensive cost-benefit analysis ought to include both the ease of use of TiProtec and the resulting lower rate of reocclusion and reoperation.

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